

## On the Influence of Cancellous Bone Structure upon the Electric Field Distribution of Electrostimulative Implants

U.Zimmermann<sup>1\*</sup>, R. Bader<sup>2</sup>, U. van Rienen<sup>1</sup>

### Motivation

- At the University of Rostock, an electrostimulative total hip revision system is being developed to support the regeneration of bone tissues as described by Basset et al. [1].
- In previous works the macroscopic electric field distribution has been investigated using a layered bone model consisting of cortical and cancellous bone.
- However, cancellous bone forms a spongy or trabecular structure which aligns along the main stress directions.
- In the present work, the behavior of the electric field within this microstructure is being investigated.



Fig. 1: Prototype of an electrostimulative acetabular cup

### Preparation of the $\mu$ CT sample for COMSOL

- In previous works, bone samples have been taken from the femoral head and mapped using micro computer tomography ( $\mu$ CT) [2].

- Height: 13 mm
- Diameter: 12 mm
- Voxel edge size: 26  $\mu$ m

⇒ 500 slices with 475 x 475 pixel  
⇒ 112.8 million voxels

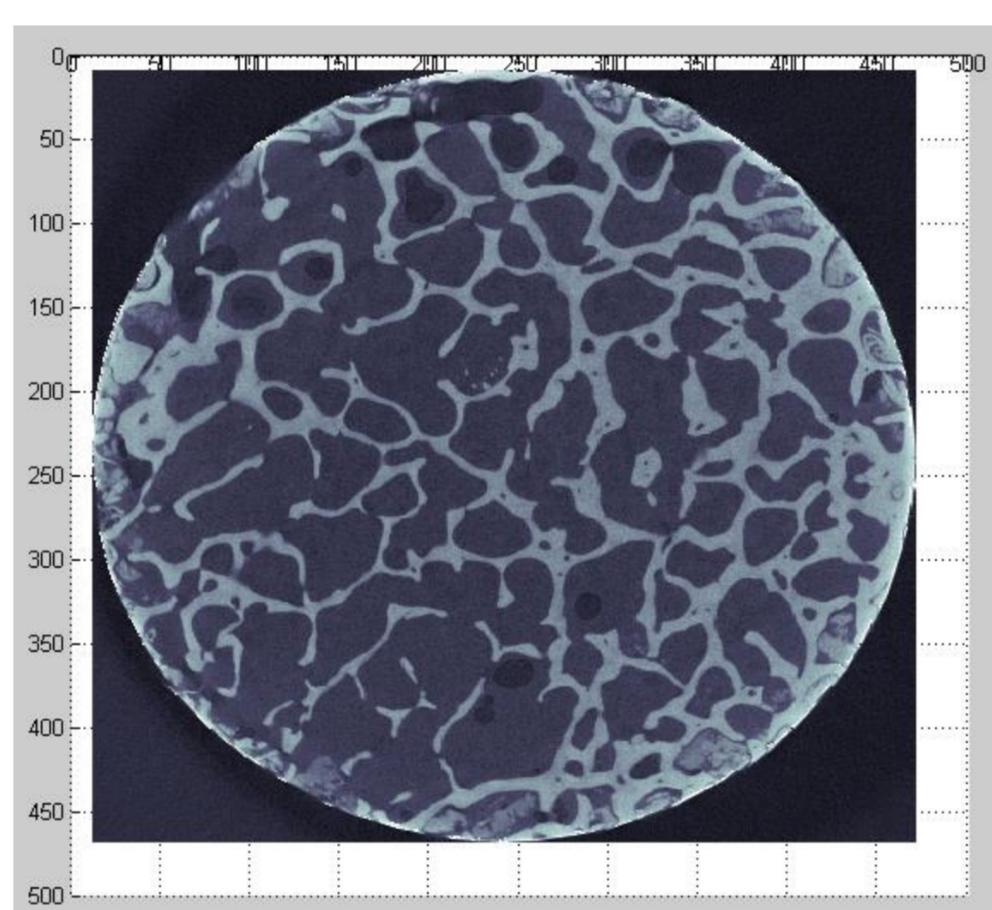


Fig. 2: Matlab illustration of one slice of the  $\mu$ CT after reduction of the edges

- At each data point the absorption of the x-ray correlates with the density of the material (Fig. 2, Tab. 1).

- The absorption is represented by a 16-bit unsigned integer number (brightness value).

- Using MATLAB®, the edges have been minimized and data points were saved to a ASCII text file using the grid data format.

- File size: 638 MB

Material	Content
Water	10 % - 25 %
Inorganic materials (Mostly hydroxyapatite)	45 % - 55 %
Organic materials (Mostly Collagen I)	Rest

Tab. 1: Material contents in cancellous bone [3]

### Definition of the COMSOL model

- Using COMSOL Multiphysics® 4.4 the electric currents interface has been used to conduct a stationary study.

- **Geometry:** Cylinder (smaller cylinder to avoid disturbances due to the drilling)

- Height: 13 mm (11 mm)
- Diameter: 12 mm (11 mm)

- **Material:** Mathematical equation including the locally changing brightness value from the previously generated text file.

- **Sources:** Terminals at the upper and lower boundary of the cylinder providing an overall voltage of: 0.91 V (0.77 V)

⇒ These sources provide a constant electric field of 70 V/m within a homogeneous tissue.

- **Mesh:** customized tetrahedral mesh resulting from a convergence analysis

- **Solver:** GMRES-Solver with ILU-Preconditioner

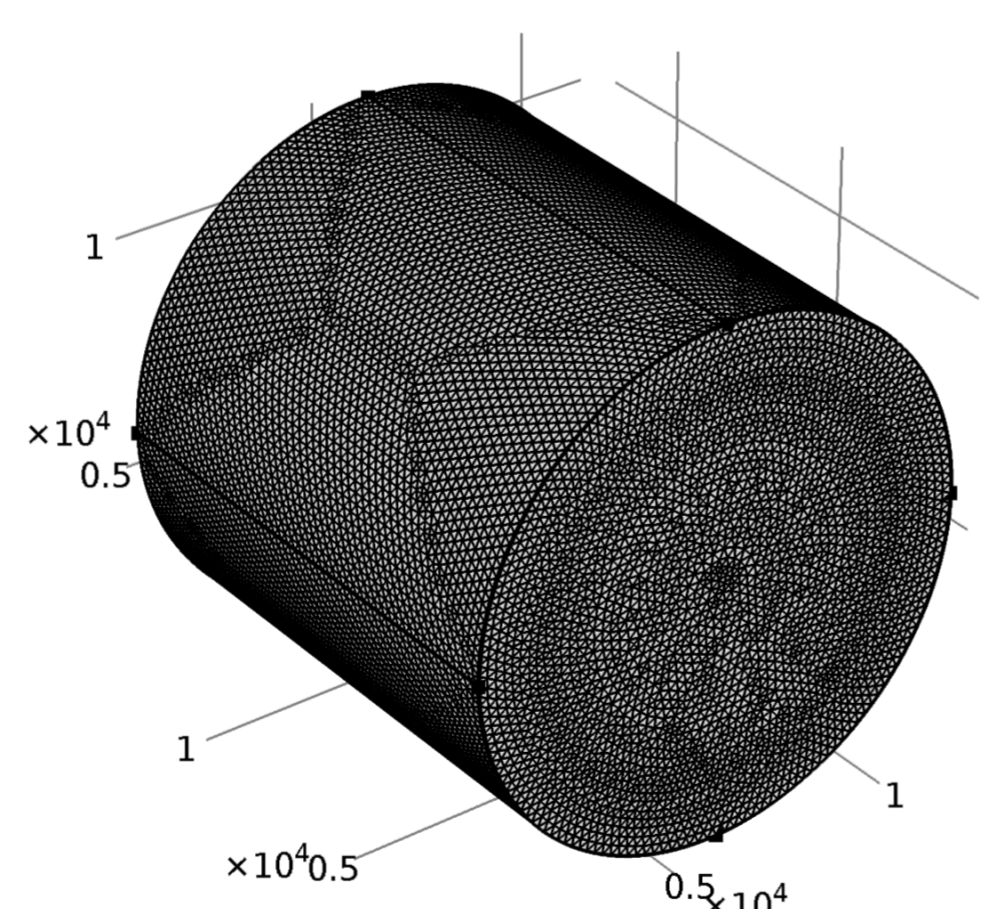


Fig. 3: Predefined "extremely fine" tetrahedral mesh: 1,699,959 mesh cells

### Basic idea

- Each brightness value represents a certain mixture of different bone tissues with a certain electrical conductivity.

- The goal of this study is to correlate each brightness value with a conductivity basing on values from literature (Fig. 4).

- Brightness values above 25000 are supposed to be pure hydroxyapatite with a conductivity of 0.

- Brightness values below 10527 are supposed to include the voxels in the corners of Fig. 2 ( $1-n/4$  of all voxels). For this reason they are neglected.

- Different approaches are used to correlate the locally changing Brightness value  $B(x,y,z)$  with the electrical conductivity  $\sigma(x,y,z)$ , where  $\alpha$  and  $\beta$  are parameters to reach certain conductivities from literature:

- Linear approach:  $\sigma(x,y,z) = -\alpha \cdot B(x,y,z) + \beta$

- Exponential approach:  $\sigma(x,y,z) = 0.002 \cdot 10^{\alpha \cdot (-\frac{B(x,y,z)}{\beta} + 1)}$

- Sigmoidal approach (Fig. 4):  $\sigma(x,y,z) = 0.75 \cdot \left( \frac{B(x,y,z) - \beta}{\sqrt{\alpha + (B(x,y,z) - \beta)^2}} + 1 \right)$

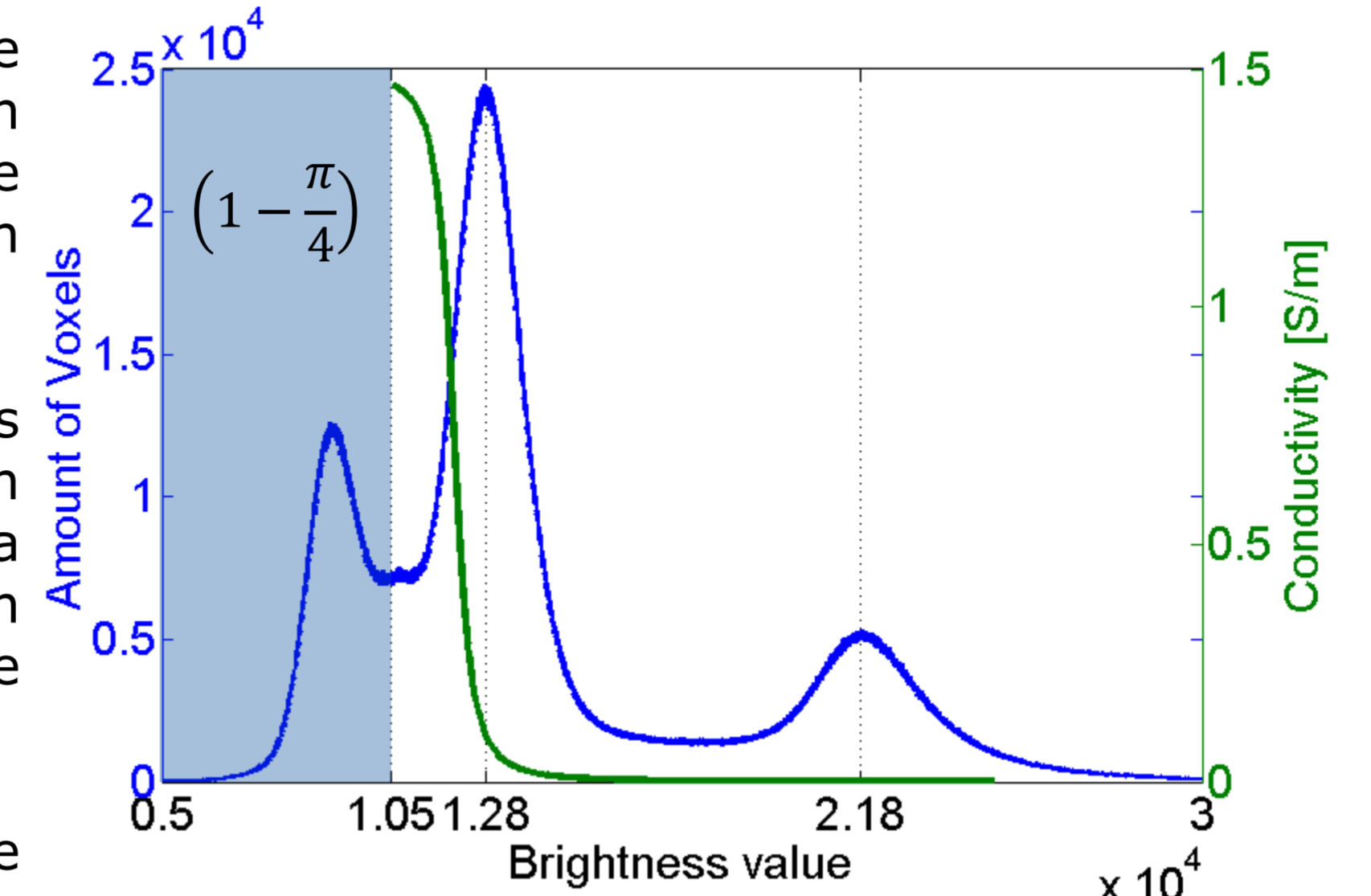


Fig. 4: Amount of voxels with a certain brightness value (blue) and correlation with the conductivity using a sigmoidal approach (green)

### Results

- Using the parametric sweep  $\alpha$  and  $\beta$  are investigated to match certain values from literature:

- Collagen I at a brightness value of 12800.
- Cancellous bone for the whole sample.

- The steeper the slope of the correlation graph for the conductivity, the bigger the deviations from the expectancy value of the electric field (Compare Fig. 6 with Fig. 7).

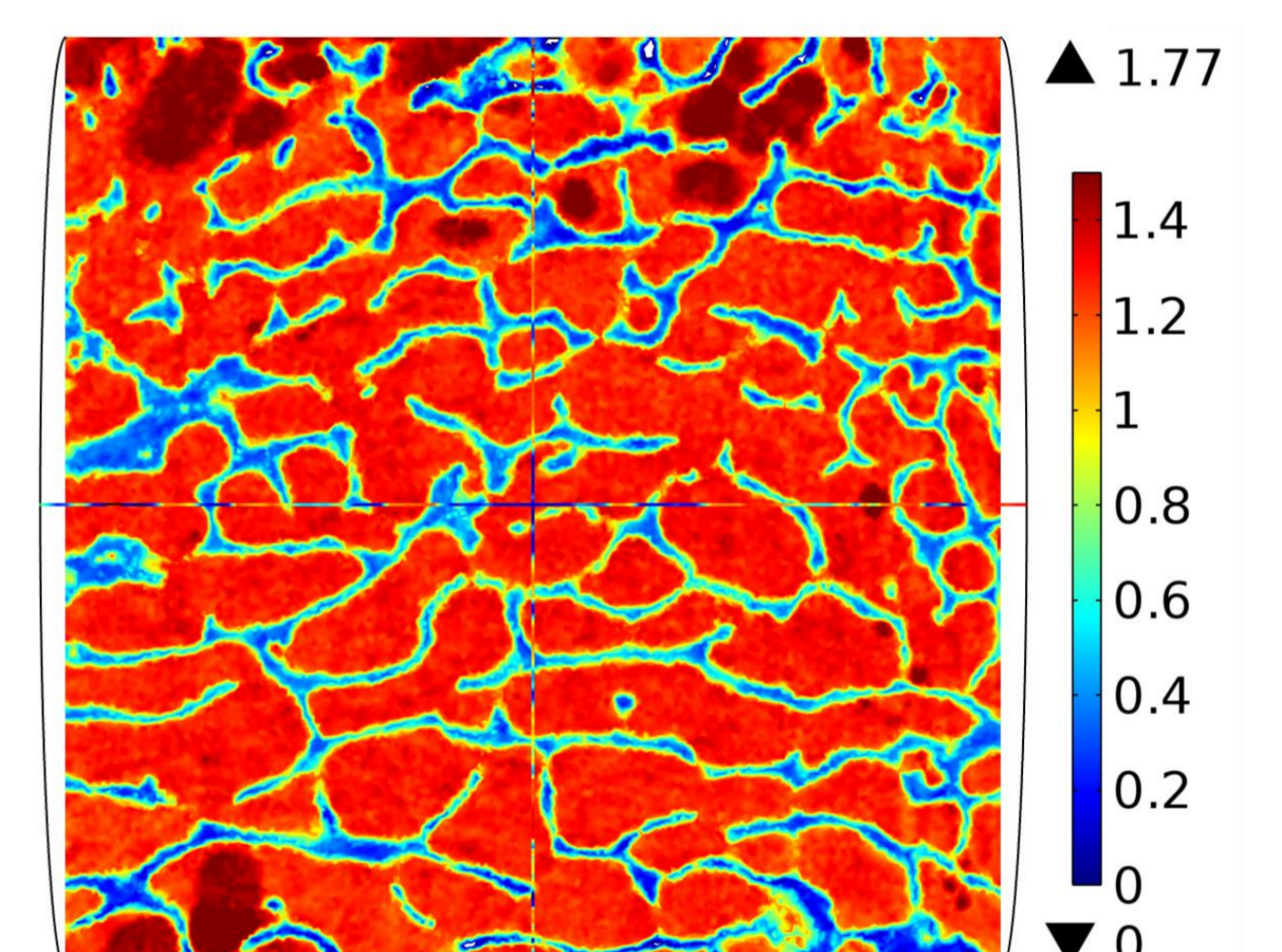


Fig. 5: Conductivity distribution [S/m] within the sample using the linear approach without consideration of conductivity values from literature

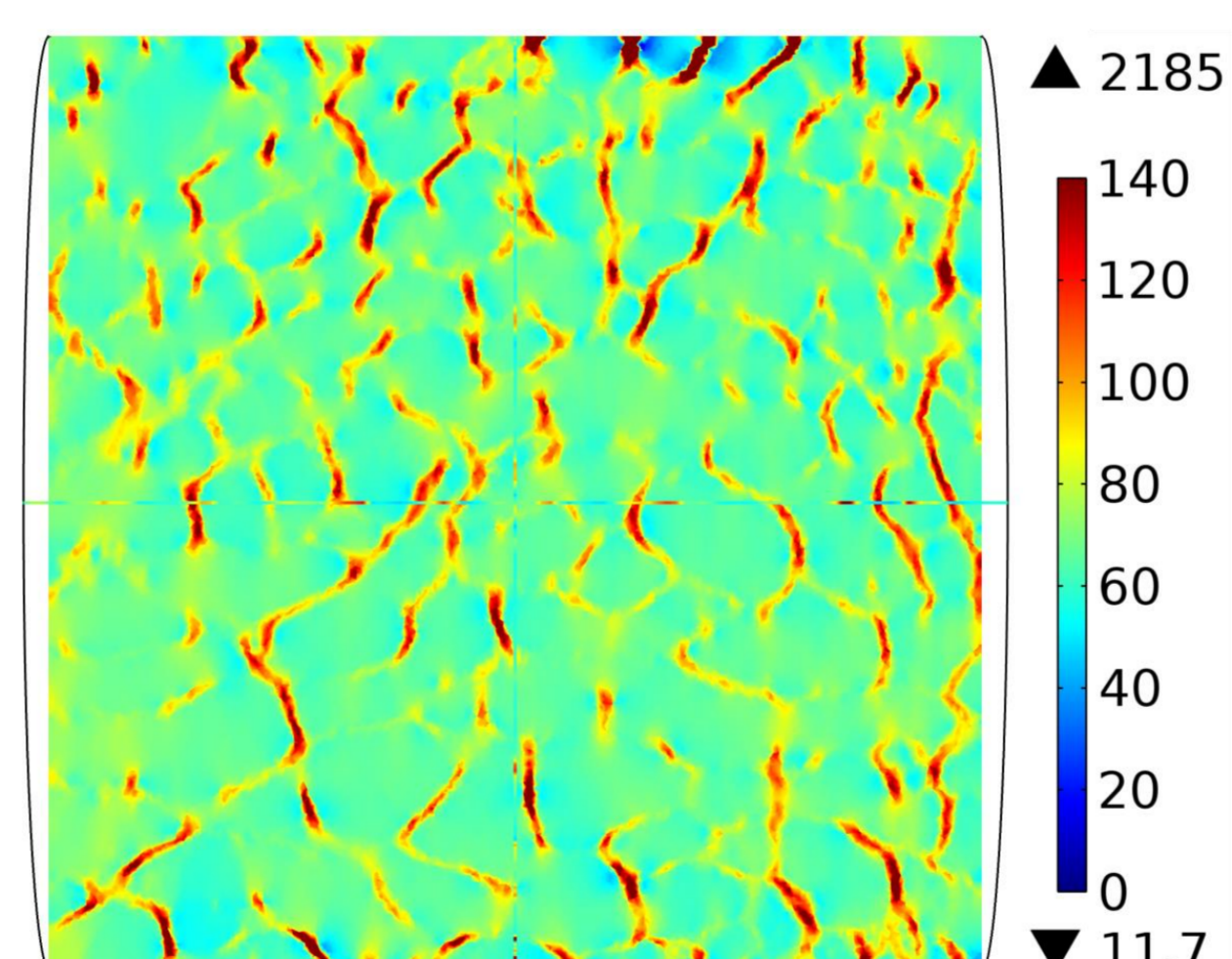


Fig. 6: Electric field distribution [V/m] within the sample using the linear approach. 70 V/m (green) is the expectancy value

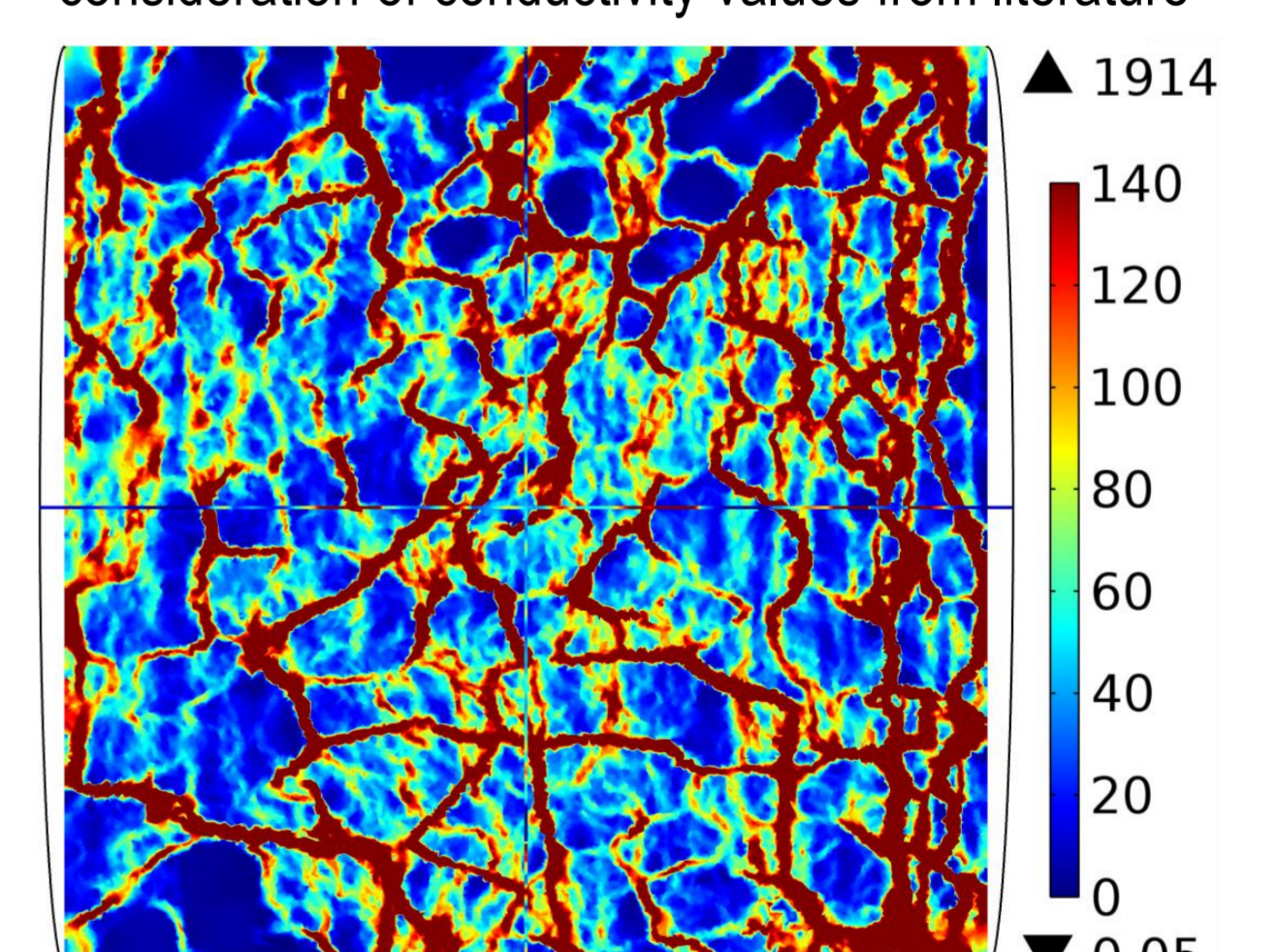


Fig. 7: Electric field distribution [V/m] within the sample using the sigmoidal approach considering literature values for collagen I as well as for cancellous bone averaging over the whole sample

### Acknowledgement

The work was supported by the DFG (German Science Foundation) Research Training Group 1505 "welisa".



Reverences:  
[1] C.A.L. Basset, R.J. Pawluk, A.A. Pilla: "Acceleration of fracture repair by electromagnetic fields" *Annals of the NY Academy of Sciences*, vol. 238, pp 242 - 262, 1974.

[2] Y. Haba, R. Skripitz, T. Lindner et al.: *Bone Mineral Densities and Mechanical Properties of Retrieved Femoral Bone Samples in relation to Bone Mineral Densities Measured in the Respective Patients*. In: *The Scientific World Journal*, vol. 2012 (20129), pp 1 - 7, 2012.

[3] DoITPoMS, J. Capes, C. McCloskey: *Structure and composition of bone*. <http://www.doitpoms.ac.uk/tiplib/bones/structure.php> (07-30-2014), DoITPoMS, University of Cambridge, 2010.

<sup>1</sup>Institute of General Electrical Engineering, University of Rostock, Albert-Einstein-Str. 2 | 18059 Rostock

<sup>2</sup>Department of Orthopaedics, University Medicine Rostock, Doberaner Str. 142 | 18057 Rostock

\*ulf.zimmermann@uni-rostock.de